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6. Abstract This paper describes altitude chamber experiments conducted with human subjects using a new continuous-flow disposable passenger mask applicable for emergency use to maximum altitudes of 41,000 feet. This mask design differs in configuration from the previous omni-directional mask designed to meet the requirements of National Aerospace Standard 1179 and FAA Technical Standard Order C-64 in that the inner face lap or seal has been eliminated and the cylindrical shape reduced to a modified one. The primary goal of this study was to determine if design modification of the mask induced an increase or decrease in physiological efficiency. Of paramount concern was the possibility that modification of the configuration and facial seal might increase the leakage rate of ambient air into the mask, and thereby compromise its ability to provide the level of protection required at the maximum altitude of the aircraft. Subjects were instrumented to obtain a variety of physiological data. This included EKG impedance pneumograph, ear oximetry, and expiratory nitrogen, and minute volume. The continuous flow of oxygen delivered to the passenger mask was controlled and precisely measured. The mask was evaluated at altitudes of 14,000, 18,500, 29,000, 35,000 and 40,000 feet. The average inspired tracheal oxygen partial pressure remained above 83.8 mm Hg under all conditions of rest and exercise at all altitudes except for the third and last minute of exercise at 40,000 feet. If a moderate degree of physical activity is to be maintained for more than a few minutes, oxygen-flow rates should be increased commensurate with the anticipated level of activity. Larger subjects with increased body surface areas exhibit lower blood oxygen saturations and tracheal oxygen partial pressures at a standardized oxygen flow due to increased oxygen consumption.			
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PHYSIOLOGICAL EVALUATION OF A MODIFIED JET TRANSPORT PASSENGER OXYGEN MASK

Introduction

This report describes altitude chamber experiments conducted with human subjects using new Sierra Engineering Series 289-601 disposable passenger oxygen masks. These masks, applicable for emergency use to 40,000-foot altitudes, differ in configuration from the previous Sierra mask (although both are designed to meet requirements of NAS 1179 and FAA TSO C-64) in that the inner face flap or seal has been eliminated and the cylindrical shape reduced to a modified cone.

The unique characteristics of continuous-flow oxygen masks, in terms of human respiration, are frequently not well understood. Although less costly than crew masks and deceptively simple in appearance, continuous-flow passenger masks have physiological performance characteristics that are relatively complex.

Continuous-flow, phase-dilution type masks, designed to the NAS 1179 and FAA TSO C-64 requirements, employ a unique design in which the reservoir is interposed between the delivery tube and the mask. The reservoir is separated from the mask by a sensitive check valve. The continuous flow of oxygen fills the reservoir bag during the respiratory pause and exhalation. The flow also continues at the same rate during inspiration. The mask-wearer receives 100% oxygen from the reservoir during an entire inspiration unless the bag is emptied; if this occurs, a spring-loaded valve in the mask opens, and ambient air is introduced to provide sufficient volume to meet the remainder of the inspiration. The flow of 100% oxygen is provided at the most advantageous point in the respiratory cycle, the beginning of inspiration. For example, if a human subject's tidal volume is 650 cc, and the reservoir contains only 500 cc at the beginning of inspiration, the 500 cc of 100% oxygen will be inspired first and delivered to the active areas of the lungs. The ambient air valve will

then open and deliver 150 cc of ambient air, which will enter the mouth, trachea, and other "dead" or inactive spaces of the respiratory system. Upon expiration, this dead-space air is the first to exit through the exhalation valve. This process is repeated with each respiratory cycle. In normal practice, the reservoir bags are capable of containing a maximum of 1,100 cc which provides for increased tidal and minute volumes.

In summary, continuous-flow, phase dilution masks offer the following advantages:

1. Oxygen economy is afforded by use of a reservoir bag that fills and retains the oxygen flow during both the respiratory pause and exhalation.

2. At lower altitudes, reduced oxygen flow rates may be employed and the air-oxygen dilution controlled in a manner more reliable than other methods employed in constant-flow oxygen masks.

3. Oxygen concentrations approaching 100%, required at 35,000 to 40,000 feet, may be obtained with moderate and reasonable flow rates.

One basic disadvantage of all continuous-flow oxygen systems is their inability to adjust automatically to the respiratory changes associated with changes in emotional and physical activity of the wearer. A healthy young male breathing air at rest normally exhibits a (volume/breath) tidal volume of about 550 cc and a minute volume (volume/minute) of 7,700 cc. Emotional and/or physical activity may cause these values to increase greatly. Concern with this problem is reflected in the Federal Aviation Regulations Part 25 (formerly Part 4B), 25.1443,¹ which requires maintenance of a mean tracheal oxygen partial pressure of 83.8 mm Hg at a tidal volume of 1,100 cc, and a 30-liter BTPS (body temperature pressure saturated) minute volume for altitudes of 18,500 to 40,000 feet.

With the introduction of jet-transport passenger aircraft certified to operate at high altitudes, new oxygen systems and masks were designed and evaluated.^{2,3} Subsequently, standards for passenger oxygen masks were compiled and published. The National Aerospace Standard 1179⁴ and Federal Aviation Administration Technical Standard Order (TSO) C-64⁵ set forth manufacturing, material, and testing standards for passenger oxygen masks.

An excellent description of the basic physiological rationale of oxygen equipment design for aircraft has been prepared by the SAE A-10, Aircraft Oxygen Equipment Committee.⁶ An additional report delineates the basic criteria and design philosophy of jet transport passenger oxygen systems.⁷

II. Methods

Procedure. The altitude chamber flight profile is shown in Figure 1. Six subjects who had received altitude indoctrination within the past

two years were employed. Instrumentation is shown in Figures 2 and 3. The mask was not donned until after air-breathing baselines were established at 10,000 and 14,000 feet. A safety observer accompanied each subject.

A Waters ear oximeter, Model XE 350, was affixed to the antihelix of the subject's ear 10 to 15 minutes prior to the chamber flight, to allow stabilization. The output of the earpiece was fed into an XE-350 oximeter and continuously recorded on a Physiograph. The latter was also used to record signals from EKG electrodes and the output from impedance pneumograph electrodes attached to the subjects. The impedance pneumograph was included in the experiment to attempt to determine if changes in the respiratory activity baseline occurred during subsequent ascent to altitude. At the present time there is no satisfactory method of measuring respiratory volumes and activity while wearing a passenger mask without compromising the performance of the mask.

After a preliminary assurance of the subject's capability to equalize ear pressures, the subject rested quietly at 10,000 feet until the ear oximeter reading indicated a stabilization of blood oxygen saturation. Then the subject was depressurized to 14,000 feet to establish similar resting air exercise baselines at this altitude.

When it appeared the blood saturation was stabilized at 14,000 feet, the subject donned crew-type demand oxygen mask and commenced breathing 100% oxygen. Immediately following crew-mask donning, exercise on a bicycle ergometer (modified so that it could be operated by each subject while seated in a passenger type aircraft seat) was initiated. The exercise level was set at 45 rpm (speed) and 45 watts (load) to obtain the desired respiratory activity (approximately 25 to 30 liters/minute). This was regarded as a light to moderate work load and approximately equivalent to walking at 3.0 to 4.0 mph.

Exercise was continued until the desired minute volume, as indicated by a dry gas meter, was obtained and stabilized. The subjects became denitrogenated during this period, thereby reducing the possibility of bends with exercise at the subsequent higher altitudes.

After completion of nitrogen washout at 14,000 feet, the subject removed the crew mask and

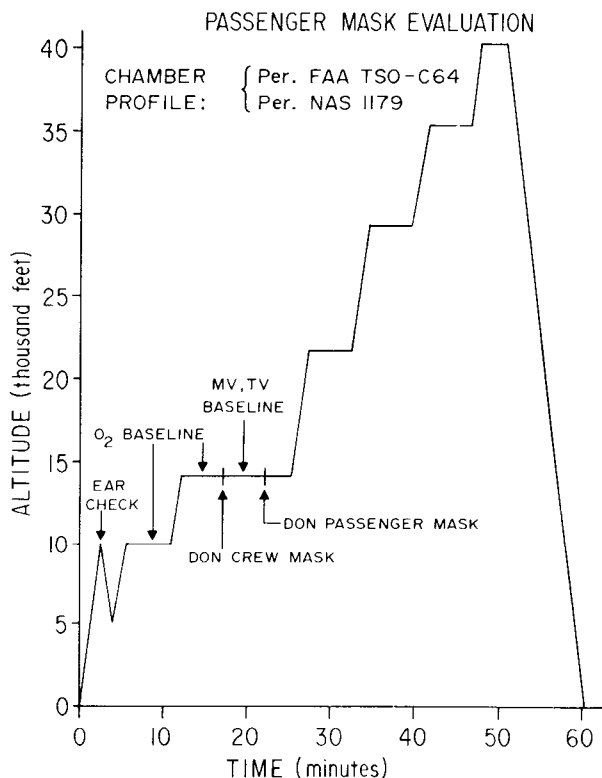


FIGURE 1. Altitude chamber profile used in evaluation of the Sierra 239-601 series prototype disposable passenger oxygen mask.

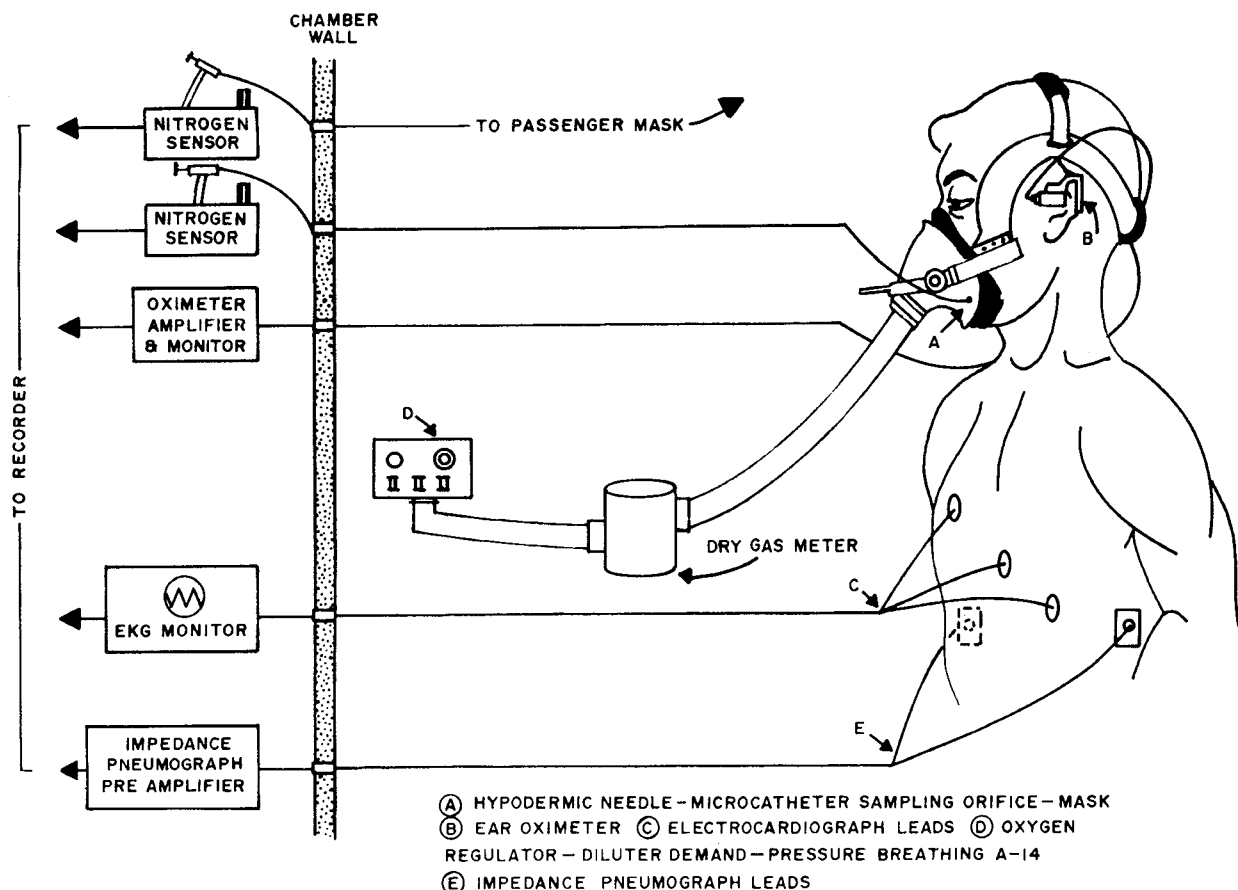


FIGURE 2. Instrumentation of subjects prior to nitrogen washout and determination of minute volume at an altitude of 14,000 feet. Subject wearing a crew-type mask.

apidly donned the Sierra passenger mask (Figure 3). Each subject wore a new mask; thus six masks were used in this evaluation. The flow of oxygen to the mask was regulated by an altitude-sensitive regulator of the type used in multi-passenger oxygen systems of transport aircraft. The flow from this regulator, instead of being transmitted directly to the subject, was first routed outside the chamber through a flowmeter and needle-valve arrangement in order to obtain precise measurement and control of the flow (Figure 3). Excess oxygen as provided by the regulator was vented outboard outside the chamber.

The subject exercised for three minutes at each altitude and rested during the climb to each successive higher altitude level. The chamber was leveled off at 14,000, 21,500, 29,000, 35,000 and 40,000 feet and readings were taken pre-exercise, during the first minute and last minute of exercise followed by post-exercise recordings

at 14,000, 21,500, 29,000, 35,000 and 40,000 feet. Motion pictures were taken of the subjects during the maximum altitude portions of the flights and closed-circuit television was used to monitor the subjects at all times.

Mask Efficiency. Two Custom Engineering and Development Company Model 300 AR Nitralyzers were used to continuously measure the mask nitrogen. These instruments exhibit an initial response latency of 0.024 second, 90% response being obtained in 0.044 second. A vacuum pump, regulated to 0.6 mm, set the sampling rate at 3 cc per minute. The continuous sample was drawn through a needle valve and microcatheter tubing (PE 60) of 0.030 inch internal diameter. The small, extremely lightweight, microcatheter tubing connected to the mask did not require extensive modification of the mask nor did it add significant weight; thus, fit and operational characteristics of the mask were not compromised.

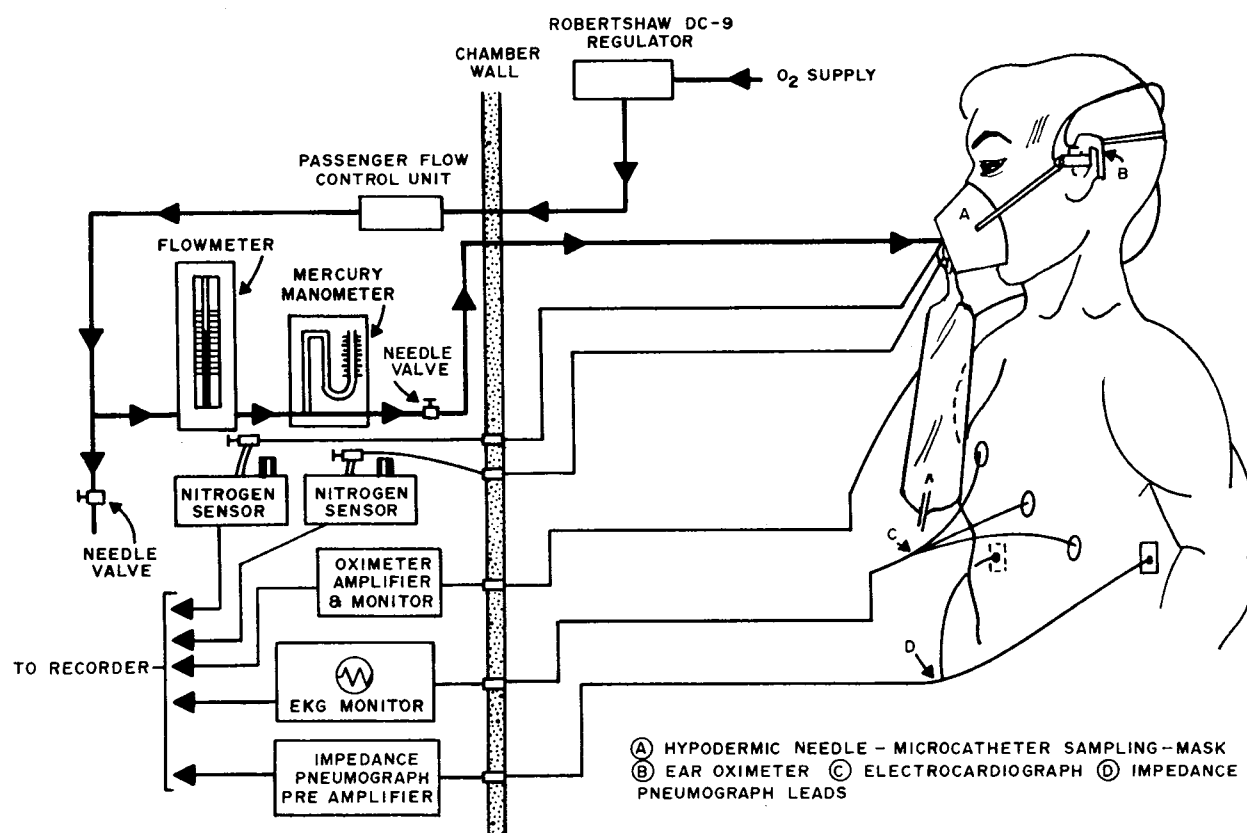


FIGURE 3. Instrumentation of subjects following completion of nitrogen washout and determination of minute volumes. Subject has completed passenger mask-donning. Oxygen flow to the mask was routed from a pressure control regulator within the chamber through the passenger flow orifices outside the chamber where it was reduced to standard conditions and returned to the mask. Excess oxygen from the regulator was dumped overboard.

In the evaluation of oxygen mask efficiency, one of the most important measurements is that of the partial pressures of inspired gases. A continuous flow mask, while worn by a human subject, defies direct measurement of these parameters (without compromise of mask performance) due to the rapid changes in gas composition at the facepiece. The percentage of gases in the facepiece of the mask may be averaged by an integrating reservoir; this average indicates a trend, but is influenced by the inactive gases of the facepiece and anatomical dead space. In order to estimate the composition of inspired gases an indirect approach was used; this technique is based on the assumption that the end-expiratory gases are completely mixed and have equilibrated with the blood in the alveoli.

Nitrogen is not involved in metabolic exchange. If the absorption of O_2 and the produc-

tion of CO_2 were exactly the same, the amount of nitrogen inspired would equal the amount expired; i.e., nitrogen molecules inspired = nitrogen molecules expired. The metabolic respiratory quotient (R.Q.) would equal one. However,

$$\text{the metabolic R.Q.} = \frac{CO_2 \text{ produced}}{O_2 \text{ consumed}} \text{ and is normally}$$

normally equal to one, or unity. Under the conditions there may be a relative difference in the nitrogen composition of inspired and expired gases. The metabolic R.Q. depends upon the predominance of carbohydrates (1.0), protein (0.82), or fat (0.71) being metabolized and is usually about 0.83. The respiratory R.Q. may vary temporarily from the metabolic R.Q. during unsteady states such as hyperventilation. The increased lung ventilation produces a blow-off of CO_2 from the blood with an apparent, lower

misleading, increase in CO₂ production and an R.Q. greater than 1.0. Conversely, hypoventilation and retention of CO₂ indicate an apparent, but misleading, decrease in CO₂ production resulting in a decreased R.Q. which may be less than 0.7.

One must keep in mind that in a steady state condition the unequal exchange of oxygen and carbon dioxide involves only that portion of the gases consumed and produced. For example, if during a one-minute period at rest 0.3 liters of O₂ were consumed and 0.25 liters of CO₂ were produced (R.Q.=0.83), the resultant volumetric difference of 0.05 liters in the seven or eight liters passing through the lungs during this one minute would be relatively small, and the error (only a few per cent) would be well within the experimental error of the determinations of end expiratory nitrogen.

All of the nitrogen which dilutes the inspired gas originates from air by mask leakage or dilution-valve activation with the exception of that derived from the tissues; after six to eight minutes of breathing oxygen under a steady state condition this constitutes less than one per cent of the lung volume.

Using calculations suggested by Luft,⁸ the admixture of air can be determined; i.e.:

$$\frac{\text{Admixture of air}}{100} = \frac{\text{Inspired nitrogen fraction}}{\text{Nitrogen fraction of air}}$$

By substituting end expiratory nitrogen for inspired nitrogen:

$$\text{Admixture of air} = \frac{\text{End expiratory nitrogen}}{\text{Nitrogen fraction of air}} \times 100$$

Using these formulas, the percentage of dilution, supply oxygen, oxygen from the ambient air, and total oxygen may be derived according to the following calculations:

$$\text{Per Cent Dilution} = \frac{\text{End expired N}_2 \times 100}{\text{N}_2 \text{ of air (79.03)}}$$

$$\% \text{ Oxygen from Supply} = 100\% - \% \text{ dilution}$$

$$\text{Oxygen from Ambient} = \text{Per cent dilution} \times \text{oxygen contained in ambient air.}$$

$$\text{Total oxygen} = \text{oxygen from supply} + \text{oxygen from ambient air.}$$

$$\text{Calculated inspired oxygen partial pressure} = \frac{(P_B - 47)}{\text{x Per cent total O}_2}$$

Where: P_B=Total pressure in mm Hg at ambient altitude.

47=Pressure, in mm Hg, of saturated water vapor at body temperature.

III. Results

The oxygen flow of the passenger mask NTPD (normal temperature pressure dry, 70° F.—760 mm-dry) and BTPS (body temperature pressure saturated, 37° C.—ambient—saturated) is shown in Figure 4. The flow to Subject 5 was increased at 29,000 and 35,000 feet during exercise due to a precipitous fall in blood oxygen saturation. Flows to the remaining subjects were adjusted to the minimal values, according to FAR Part 25.

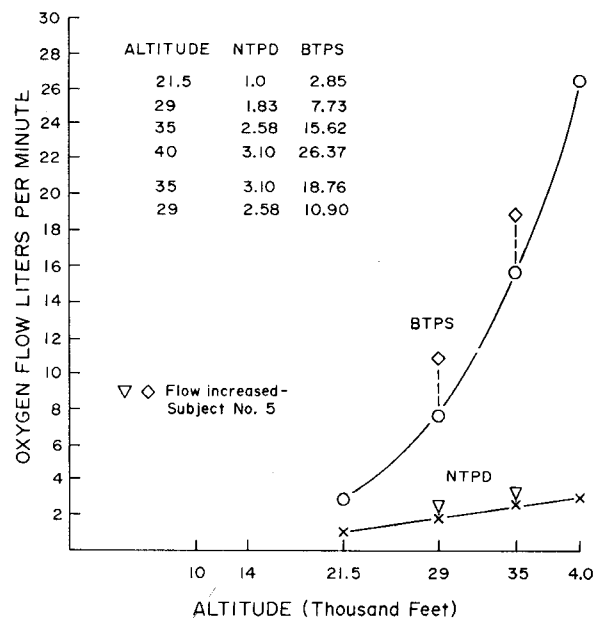


FIGURE 4. Oxygen flow rate.

Heart Rate. Predictably, the mean heart rates increased with exercise, this being more pronounced in the third minute of exercise. There was also an over-all increase in mean heart rate with increase in altitude (Figure 5). These latter increases at similar exercise levels may have been partially due to subject apprehension with increase in altitude; however, the main stimulus appears to be hypoxic stress as indicated by lower blood oxygen saturations and lower oxygen partial pressures at the higher altitudes (Figures 6 and 7). At 40,000 feet, the average tracheal oxygen partial pressure dropped from 86.4 mm Hg at the end of the first minute to 77.2 at the end of the third minute (Figure 7). A typical nitralyzer record is shown in Figure 8. The oximeter earpiece used on Subject

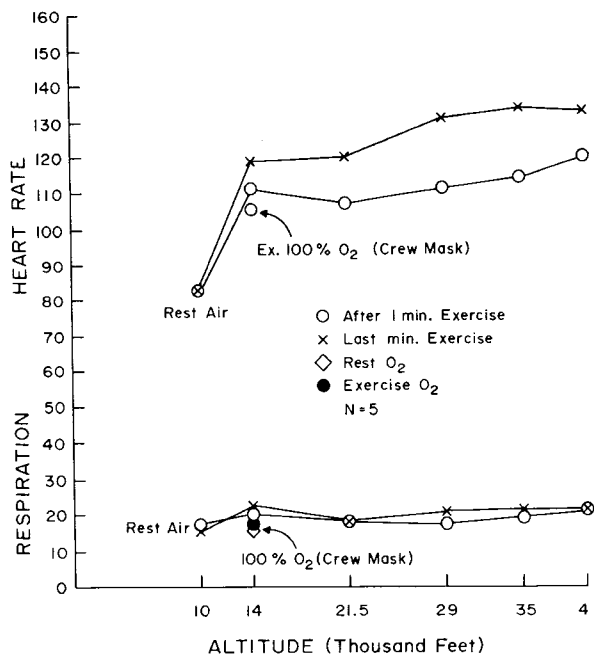


FIGURE 5. Average heart and respiratory rates. Note the increase in heart rate from the first to the last minute of exercise at altitude.

No. 1 appeared erratic and unstable with readings, for example, of 90% blood saturation while breathing 100% oxygen at 14,000 feet. The ear-piece and amplifier were replaced. The average blood oxygen saturation dropped to its minimum value at the end of three minutes of exercise at 40,000 feet (83.6%); however, re-saturation to an average of 90.8% occurred within a short period of time (30-45 seconds) following cessation of exercise (Figure 6).

Blood Oxygen Saturation. The National Aerospace Standard states that blood oxygen saturation baselines established at 10,000 and 14,000 feet should be obtained with the subject engaged at the same level of activity as during the evaluation at higher altitudes. Comparison as the mean blood oxygen saturation of the subjects at rest breathing air at 14,000 feet (93.8%) to that at the last minute of exercise (89.9%) indicates a difference of 3.9% which agrees with results obtained in a previous study.⁹ Average blood oxygen saturation levels prior to exercise exceeded the resting baseline (93.8%) at all altitudes. Post-exercise saturations were 1.3% to 4.6% lower than the above baselines.

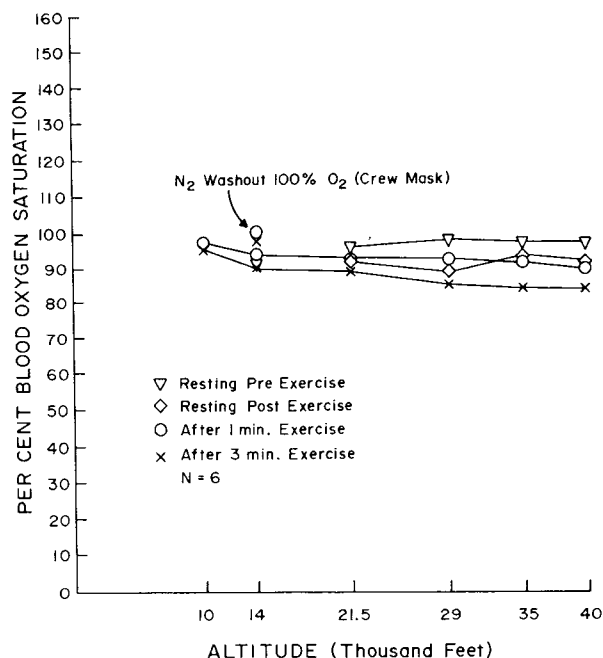


FIGURE 6. Average blood oxygen saturation as determined by ear oximetry. Note the decrease in blood oxygen saturation from the first to the third minute of exercise.

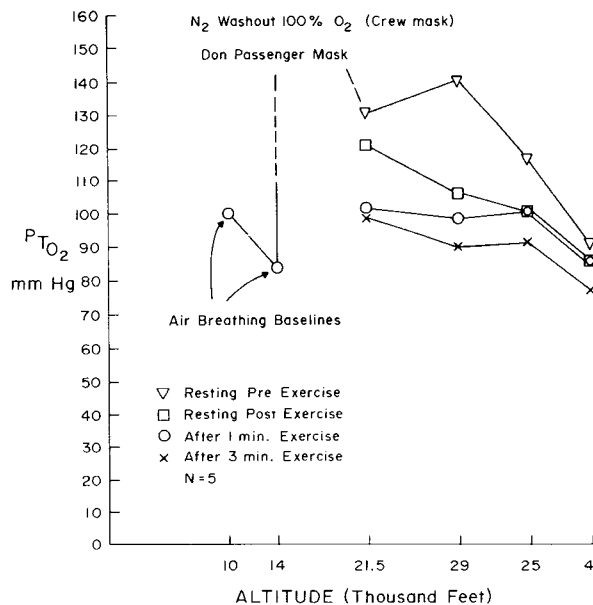


FIGURE 7. Average inspired oxygen partial pressure. The air breathing baseline at 10,000 and 14,000 feet is merely a function of barometric pressure; i.e. $(P_B - 47) \times 20.94\%$ and is identical irrespective of physical activity. The combination of a crew mask and breathing 100% oxygen at 14,000 feet causes the inspired tracheal oxygen partial pressure to go off scale to a calculated value of approximately 400 mm Hg.

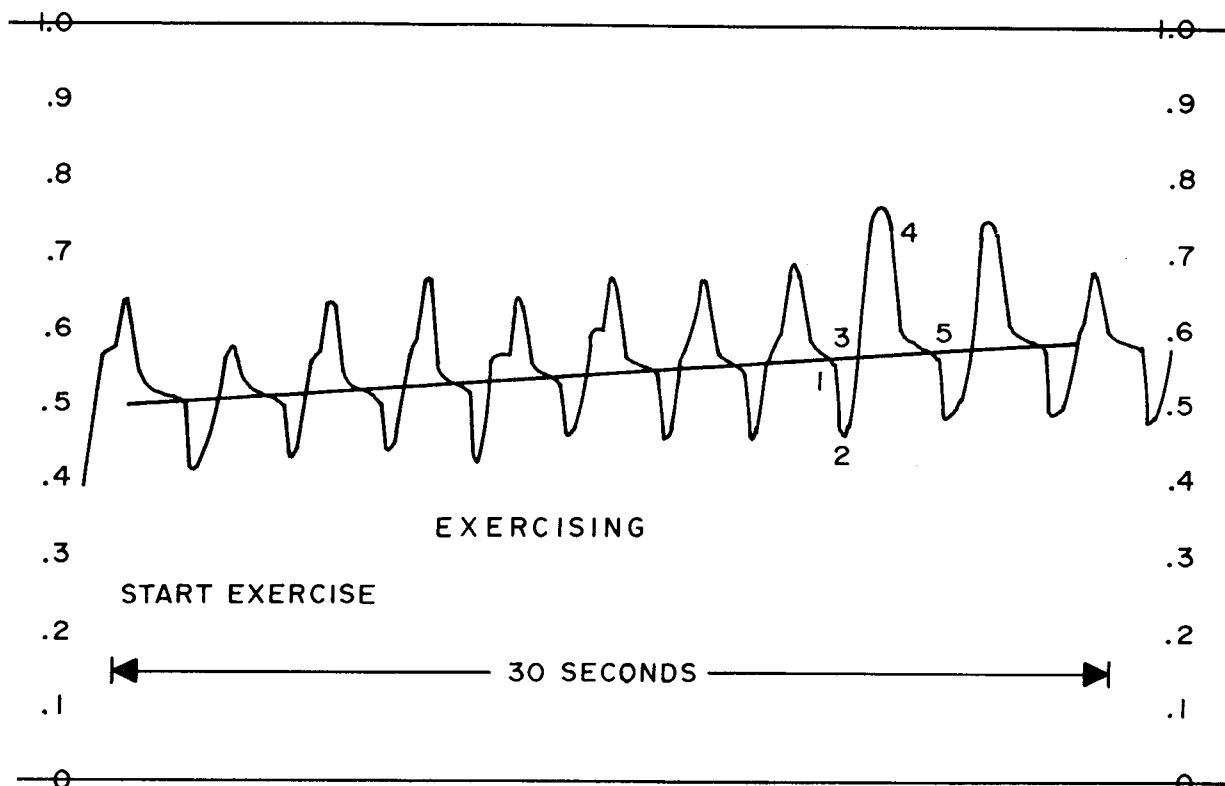


FIGURE 8. Nitralyzer record of Subject No. 4 at 29,000 feet. Slope of line indicates increased dilution and reduced $P_{T}O_2$ due to exercise. Numbers 0-1.0 equal 0-100% nitrogen subject to calibration correction. Nitrogen value should not be confused with flow, volume or mechanics of respiration. (1) Inspiration of oxygen from reservoir. (2) Dilution valve activated. (3) Continuing. (4) Oxygen, inspired primarily at (1) above, exhaled. (5) End expiratory nitrogen concentration.

Oxygen Partial Pressure. The tracheal oxygen partial pressure remained above 83.8 mm Hg in all subjects under all conditions of altitude for the first minute of exercise except for Subject No. 5, who experienced a drop in $P_{T}O_2$ to 71 mm Hg at the end of the first minute of exercise at 40,000 feet. In the third minute of exercise, the $P_{T}O_2$ of this subject dropped to 70, 71, and 64 mm Hg at altitudes of 29, 35, and 40 thousand feet, respectively. To offset the precipitous drop in $P_{T}O_2$ and blood oxygen saturation at 35,000 feet, the flow was increased from 2.58 lpm to 3.10 lpm; the post-exercise $P_{T}O_2$ climbed to 93 mm Hg and 99%. After recovery after 1½ minutes of exercise, in which the $P_{T}O_2$ and blood oxygen saturation dropped to 64 mm Hg and 80%, was accompanied at 40,000 feet by merely discontinuing exercise; this produced a rapid climb in $P_{T}O_2$ and blood oxygen saturation to 93 mm Hg at 40,000 feet.

Respiration. Subject No. 5 was the oldest (age 45) and the largest (225 lbs.) of the subjects used

in this series of experiments. His larger body surface area undoubtedly increased his oxygen consumption in comparison to the other subjects. He exhibited marked increases in respiratory rate from 14 respirations per minute at 14,000 feet (at which time the baseline minute volume was determined) to 24, 25 and 24, respectively, at 29, 35 and 40 thousand feet. A crude estimate of this effect may be made by assuming that the baseline tidal volume (determined during exercise at 14,000 feet) remained constant (1,857 cc) during subsequent ascent to higher altitudes. The indicated increase in respiratory rate would, therefore, increase the baseline minute volume from 26 lpm (BTPS) at 14,000 feet to 44.6 lpm at 29,000 and 40,000 feet, and 46.4 lpm at 35,000 feet, an overall minute volume increase of 48% to 54% above the specified lpm. With these conditions prevailing, the basic design criterion of the mask is exceeded by approximately 50%.

Subject No. 2 exhibited satisfactory $P_{T}O_2$ and blood oxygen saturation levels at the end of the first minute of exercise; however, oximetry indi-

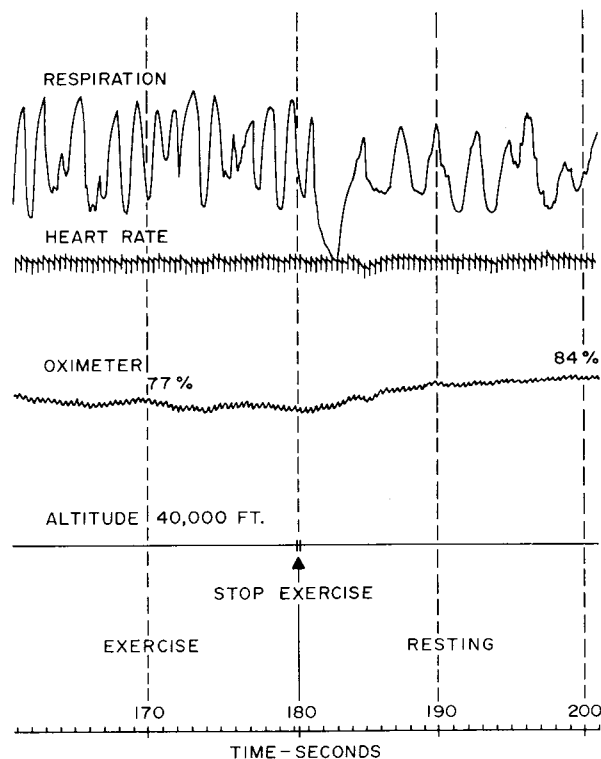


FIGURE 9. Sample. Physiograph recording showing rapid blood oxygen re-saturation following cessation of exercise at 40,000 feet. Subject No. 2.

cated a relatively low blood oxygen saturation (without a commensurate lowering of tracheal oxygen partial pressure) at the end of the third minute at 29, 35, and 40 thousand feet. Rapid recovery of blood saturation following cessation of exercise is shown in a sample recording from this subject (Figure 9). This subject did not exhibit a marked change in respiration when compared to the 14,000-foot baselines; however, he exhibited one of the most consistently elevated heart rates during exercise at 35 and 40 thousand feet, which may be indicative of his response to hypoxic stress, state of physical condition, or both.

IV. Discussion

The National Aerospace Standard (NAS) recognizes gas analysis and blood-oxygen-saturation determination as the two principal alternate methods to be used in altitude-chamber evaluations of passenger masks.

In this study, the experiments were designed to measure both of these variables simultaneously.

Exercise time at altitude was held to a minimum in order to minimize the probability of bends and to reduce fatigue.

Previously, high altitude evaluations of passenger masks have been carried out on resting subjects. In some evaluations, a brief episode of voluntary hyperventilation took place to increase minute volumes to 30 liters/minute. This procedure is recommended in NAS 1179, but is practically impossible for a sedentary subject to maintain this level of respiration for more than 30 to 45 seconds without experiencing severe symptoms of hypocapnia (dizziness, paraesthesia, muscular cramps, etc.).

In addition, voluntary hyperventilation reduces the alveolar and blood carbon dioxide partial pressures by the washout effect. By mere physical reduction of the carbon dioxide partial pressure, an increase in alveolar oxygen partial pressure is induced. As pointed out previously, this physiologically unsteady state may be maintained for only brief periods. Changes in blood chemistry and cerebral blood flow induced by voluntary hyperventilation detract from its usefulness in mask evaluation.

A controlled and measured work load was used in these experiments to stimulate respiration to the 30 liters/minute standard with imposing severe changes in respiratory blood-gas composition.

Admittedly, increased work load produces an increase in oxygen consumption. The level of work load used in these experiments should produce an increase in oxygen consumption of approximately .35 to .50 liters/minute above resting value.¹⁰

Neither voluntary hyperventilation nor exercise is entirely a satisfactory means of elevating the minute volume; voluntary hyperventilation tends to over-estimate the physiological effectiveness of a mask, and exercise tends to underestimate this value. The use of exercise, however, increases the margin of safety and assures that an adequate blood oxygen saturation can be maintained during periods of increased respiration.

One disadvantage of using exercise in mask evaluations at altitude is the increased susceptibility to the development of bends. The depth of denitrogenation, altitude profile, and exposure time must be carefully considered in relation to the use of exercise.

The increased minute and tidal volumes developed during exercise impose efficiency requirements of mask performance in excess of similar valuations conducted on the sedentary, resting subject.

At 40,000 feet, 3.1 liters/minute NTPD equals 3.4 liters/minute BTPS. A subject breathing 0 liters/minute will empty the reservoir bag and raw in air through the ambient air valve. The average composition of inspired gas is shown in figure 10.

If, however, there are significant and uncontrolled openings around the periphery of the mask, ambient air may be drawn through these during peak inspiration rather than through the check valve of the reservoir bag.

The ear-oximeter determinations exhibit some degree of variability, depending upon physical activity and subject movement. Fluctuation of the ear oximeter was pronounced during resting and air breathing at 14,000 feet, became more stable with 100% oxygen and exercise at 14,000

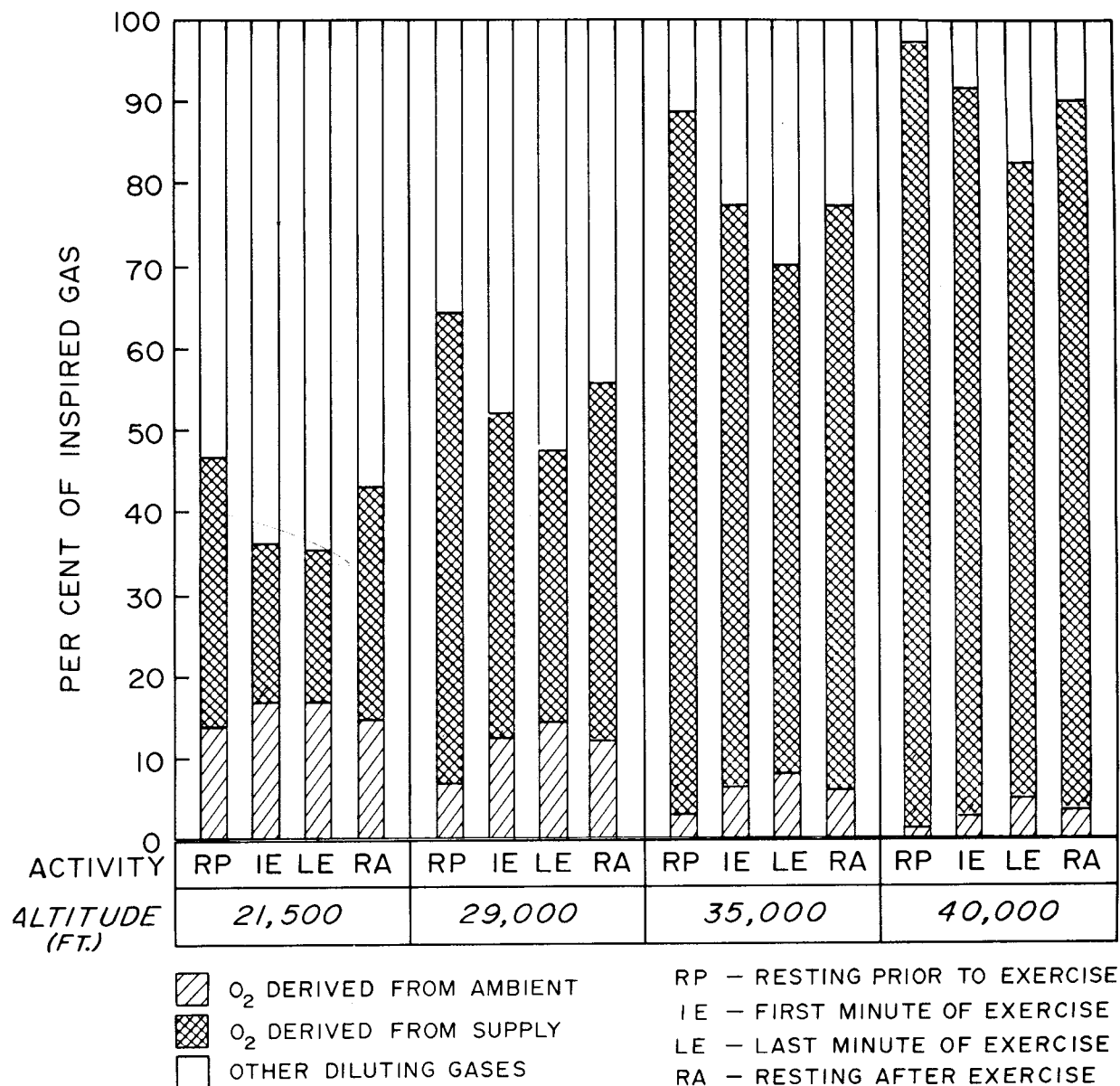


FIGURE 10. Histogram showing dilution of inspired gas with ambient air as calculated from the end expiratory nitrogen concentrations.

feet, and again fluctuated to a marked degree at 40,000 feet on oxygen. It appeared that this "hunting" phenomenon was more marked when some degree of hypoxia was present. In general, the ear-oximeter readings appeared to be more stable during exercise than at rest.

Maintenance of an adequate blood-oxygen saturation is the desired end result. Instrumentation artifacts and variations in the physiological response of the mask-wearer may result in considerable variation in the ear-oximetry indications of blood-oxygen saturation.

The function of the mask is to deliver sufficient oxygen to produce an adequate tracheal oxygen partial pressure. Since pressure breathing is not involved in passenger systems, the mask cannot provide partial pressures in excess of those provided by a 100% concentration of oxygen. A hypothetical leak-free passenger mask, capable of delivering undiluted 100% oxygen to the alveoli throughout inspiration would therefore exhibit maximum efficiency. The resulting oxygen partial pressure, therefore, becomes merely a function of the ambient barometric pressure minus the vapor pressure of saturated gas inspired, i.e.: $(P_B - 47)$.

It should be pointed out that a discrepancy exists between the performance of any oxygen equipment evaluated at constant altitude, as presented in this report, and the dynamic changes which occur during rapid decompression. Experiments have been conducted in this area by Bryan and Donaldson,^{11 12} but are beyond the scope of this report.

V. Conclusions

1. The average inspired tracheal oxygen partial pressure remained above 83.8 mm Hg under all conditions of rest and exercise at all altitudes except for the third (last) minute of exercise at 40,000 feet.

2. The average blood oxygen saturation during exercise remained above the 14,000-foot air breathing baseline (90.8%) during the first

minute of exercise except at an altitude of 40,000 feet where it dropped to 89.6%.

3. Following three minutes of exercise, mean blood oxygen saturation dropped below the 14,000-foot air breathing control baselines at altitudes by differences of 0.7, 4.8, 5.9, and 6 per cent at 21.5, 29, 35 and 40 thousand feet respectively.

4. The average respiratory rate at the maximum altitude increased 20% during the first minute of exercise, and 37% during the last minute of exercise when compared to baseline minute volumes determined at 14,000 feet breathing 100% oxygen. Providing tidal volumes remained constant, the mean volumes would approximate 28.8 to 32.8 liters/minute. There were large individual variations, however, with the 30 lpm minute volume requirements of TSO C-64 being exceeded by as much as 50%.

5. As in previous evaluations^{13 14} larger subjects with increased body surface area exhibit lower blood oxygen saturations and tracheal partial pressures at a standardized oxygen flow due to increased oxygen consumption.

6. An ideal technique for increasing the respiratory minute volume to the levels specified NAS-1179 and TSO C-64 is not readily attainable. Originally formulated by general consensus of a number of physiologists, physicians, and engineers, these levels are representative of anticipated minute volume that a naive passenger would exhibit during the excitement of aircraft rapid decompression.

7. Voluntary hyperventilation leads to overestimation of the efficiency of a mask design whereas evaluation during exercise underestimates mask efficiency within the framework and intent of NAS 1179 and the Federal Aviation Regulations.

8. If a moderate degree of physical activity is to be maintained for more than a few minutes oxygen flow rates should be increased commensurate with the anticipated level of activity.

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